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Radiotherapy Application of High-Density Laser Wakefield Acceleration (LWFA)

T. Tajima^a and D. Roa^b

^a Department of Physics and Astronomy, ^b Department of Radiation oncology

University of California at Irvine , CA, 92697 USA



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Wake acceleration



Bow wake and stern wake Nature (or mother duck) shows us.





Theory of wakefield toward extreme energy



Demonstration (1994), realization, and applications



(2004)



4 GeV laser accelerator LBI



(Michigan)

29 MAY 1995

Nakajima, et al (1994, 1995)

Relativistic vs Nonrelativistic LWFA

1. High phase velocity paradigm: Tajima-Dawson (1979) $v_{ph} \rightarrow$ large (close to c)

VS

2. Relativistic amplitude of LWFA :

*a*₀ > 1

3. Relativistic coherence (Tajima, 2010)

Strong beam (of laser / particles) drives plasma waves to saturation amplitude: $E = m\omega_p v_{ph}/e$ **Relativistic coherence** enhances beyond the Tajima-Dawson field: $E = m\omega_p c a_0/e$ (~ GeV/cm) No wave breaks and wake <u>peaks at relativistuic regime</u> <u>v≈c</u> Wave breaks at v<c at non-relativistic regime</u>

Relativistic coherence (Tajima, 2010)

Nonrelativistic cases (today: more to follow)





 $a_0 > 1$



*a*₀ < 1

Laser Wakefield (LWFA):

Wake phase velocity >> water movement speed maintains coherent and smooth structure



VS

Tsunami phase velocity becomes ~0, causes easier trapping and acceleration of more #



Strong beam (of laser / particles) drives plasma waves to saturation amplitude: $E = m\omega v_{ph}/e$ No wave breaks and wake <u>peaks at v~c</u> Multiple of waves at v < c





With low phase velocity More particle trapping

Transition to $a_0 < 1$ regime Transition to near-critical density $n_e \sim n_{cr}$



Laser Wakefield Acceleration near critical density

Near critical density ~ n_e = 10²¹/cc

gaseous plasma \rightarrow solid nanotube

Excitation of electron acceleration possible with $I \sim 10^{14} \,\text{W} / \text{cm}^3$

Coupling gets stronger near $n_e = 10^{21}/\text{cc}$ \leftarrow overlap of plasma waves with different v_p \leftarrow curved laser ω (k), varied v_a





Dispersion Relation: FFT(Log₁₀E)

High Harmonic Generation

 Short Wavelength and Low Phase Velocity Electrostatic Waves allow for more efficient particle acceleration



Laser beat wave excitation of wakefield

Beat of two lasers $(\omega_0 k_0)$ (ω_1, k_1) to match with the plasma eigenmode $(\omega_p, k_0 - k_1)$, \rightarrow wakefield



$$v_{ph} = \frac{\omega_p}{k_p} = \frac{\omega_0 - \omega_1}{k_0 - k_1}$$

$$v_g = \frac{\partial \omega}{\partial k} = \frac{c}{\Box} \sqrt{1 - n_e/n_c}$$

Nonrelativistic limit of energy gain

 $W_{max,nr} = \frac{\pi}{2} m v_{ph}^2 a_0^2 \left(\frac{\omega_0}{\omega_p}\right).$

Target Foil Simulations in time: $a_0 = 0.007 \rightarrow 10^{14} W/cm^2$ with 2 µm Target



Beat wave excitation of plasma wave



When $n_e \sim n_{cr}$, i..e $\omega_1 \sim \omega_p$

(E. Barraza)

Free-Space Laser vs. Fiber Laser





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Fiber laser technolo)gy
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Application	Average Power	Pulse Width	Peak Power	Spatial Mode	Focused Intensity
Metal cutting (heat)	1 to 100 kW	Continous	same as average	ММ	$10^7 \mathrm{W/cm}^2$ (CW)
Semiconductor Processing	10 to 1000 W	1 to 100 ns	MW (10 ⁶ W)	MM/SM	10 ⁹ W/cm ² (peak)
Glass cutting (cold ablation)	> 10 W	≤ 0.5 ps	Hundreds of MW	SM	10 ¹³ W/cm ² (peak)
Portable LWFA (>10 keV eletrons)	1 to 10 W	≤1 ps	\geq GW (10 ⁹ W)	SM	$\geq 10^{14}$ W/cm ² (peak)

MM: multi-mode (spatial)

SM: single mode





hollow fiber laser

Multimode pump input







CAN fiber lasers

←

Conventional electron accelerator (and X-ray) for Therapy ← 5-10m (next room) →

Electron energies by accelerator: 6-20MeV

 \rightarrow X-rays

LWFA could provide high dose <u>"FLASH</u>" therapy

Furthermore, much tinier with fiber



In situ / endoscopic fiber delivery of electron radiotherapy of cancer



Fiber laser drives in situ nanotube target in front of cancer cells

→ Compactification, accurate (no collateral damage), and cheap

Cost estimate comparison with Brachy therapies

 $\mathbf{\Lambda}$

Item	<u>LWFA – HDR</u>	Iridium-192–HDR	Cobalt-60–HDR
Purchase Estimate	\$100K - \$300K	\$700K - \$900K	\$700K - \$900K
Room Shielding	None	\$200K - \$500K	\$200K - \$500K
Source Replacement	None	~\$10K every 4-6 months	~130K every 60 months
Downtime due to Source Replacement	None	1-2 days	1-2 days

(Prof. D. Roa, preliminary estimate)

Current treatment applications (from skin, vagina, uterine, breast, etc.)



→ Much smaller, endoscopic in ours

(Prof. D. Roa)

Vector nanomolecule with high-Z metal to target cancer cells for electron radiotherapy

High-Z: stop electrons Nanomolecule vector: attached to cancer cell



Nanomolecular vector medicine, (after F. Tamanoi, 2022)

Summary

- 1. Near critical density (e.g. nanotube material) \rightarrow low phase velocity LWFA
- 2. Low energy electrons (> 10keV, < MeV), large amount with modest laser power (using Raman forward process)
- 3. Fiber laser technology (s.a. hollow fiber laser)
- 4. Endoscopic (through fiber) delivery of electrons for radiotherapy ← replacing Brachy therapy
- 5. With nanomolecule vector (with high-Z particle attached), further accuracy, focus of electrons

Recent advancements in generation of intense X-ray laser ultrashort pulses open opportunities for particle acceleration in solid-state plasmas. Wakefield acceleration in crystals or carbon nanotubes shows promise of unmatched ultra-high accelerating gradients and possibility to shape the future of high energy physics colliders. This book summarizes the discussions of the "Workshop on Beam Acceleration in Crystals and Nanostructures" (Fermilab, June 24–25, 2019), presents next steps in theory and modeling and outlines major physics and technology challenges toward proof-of-principle demonstration experiments. Chattopadhyay • Mourou Shiltsev • Tajima

BEAM ACCELERATION IN CRYSTALS AND NANOSTRUCTURES

Edited by

Swapan Chattopadhyay • Gérard Mourou Vladimir D. Shiltsev • Toshiki Tajima

Thank you very much!

BEAM ACCELERATION IN CRYSTALS AND NANOSTRUCTURES





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Appendix to p. 15:

Conventional electron accelerator for radiotherapy

